

# 'Use of compliant actuators in prosthetic foot designs'

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[http://mech.vub.ac.be/multibody\\_mechanics.htm](http://mech.vub.ac.be/multibody_mechanics.htm)



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**IEEE HUMANOIDS 2009 WORKSHOP**  
MODELING, SIMULATION AND OPTIMIZATION OF BIPEDAL WALKING

December 7, 2009, Paris, France



Vrije Universiteit Brussel



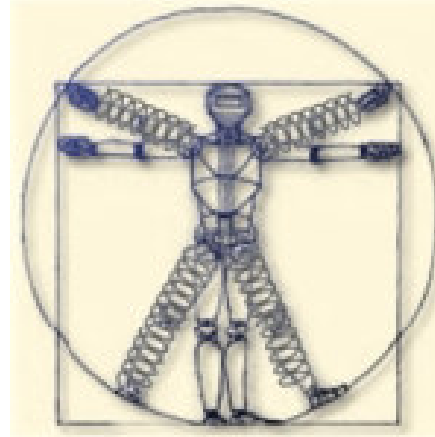
## Outline

- Introduction
- Compliant and Adaptable Compliant Actuators: working principles
- Prosthetic foot designs
- Conclusions





## Introduction



### FP7 : VIACTORS

Variable Impedance Actuation Systems  
Embodying Advanced Interaction Behaviours  
Grant agreement no.: 231554

## Review of Actuators with Passive Adjustable Compliance / Controllable Stiffness for Robotic Applications

Ronald Van Ham, Thomas G. Sugar, Bram Vanderborght, Kevin W. Hollander and Dirk Lefeber  
IEEE Robotics and Automation Magazine



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## Introduction

# Why using variable impedance actuators in humanoid walking

Efficiency : store energy during negative work; reduce the size of the motors

Cope with impact at heelstrike

'Soft' safe human robot interaction



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## Compliant Actuators

### *Active Compliant actuators*

Compliant behaviour of a stiff actuator based on software control

not inherently compliant, no impact

No energy can be stored

power is required both to accelerate and decelerate a mass.  
One motor !!!

### *Passive Compliant Actuators*

Actuators with an elastic element (spring)



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## Passive Compliant Actuators

Passive = contains an elastic element

Inherent compliance : unlimited bandwidth to absorb shocks, energy storage

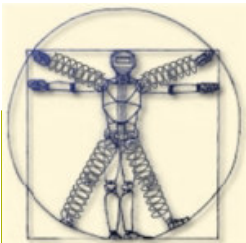
Constant compliance  $\leftrightarrow$  Variable compliance

Equilibrium controlled stiffness

Antagonistic controlled stiffness

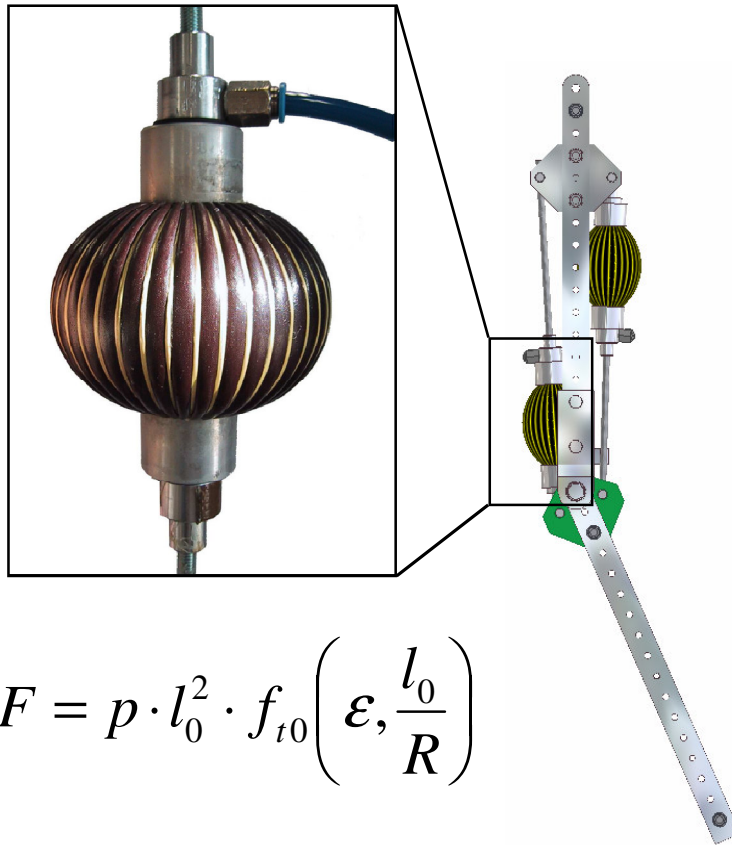
Structural controlled stiffness

Mechanically controlled stiffness





## Antagonistic Controlled Stiffness



$$F = p \cdot l_0^2 \cdot f_{t0} \left( \epsilon, \frac{l_0}{R} \right)$$

- Pleated membrane
- Low weight (< 150 g !)
- High force levels
  - ⇒ up to 3000N at 3 bar
- Inherent compliance
- Graceful degradation
- No threshold pressure
- Direct joint attachment
  - ⇒ no gear reduction, no backlash
- Bidirectional rotative actuator



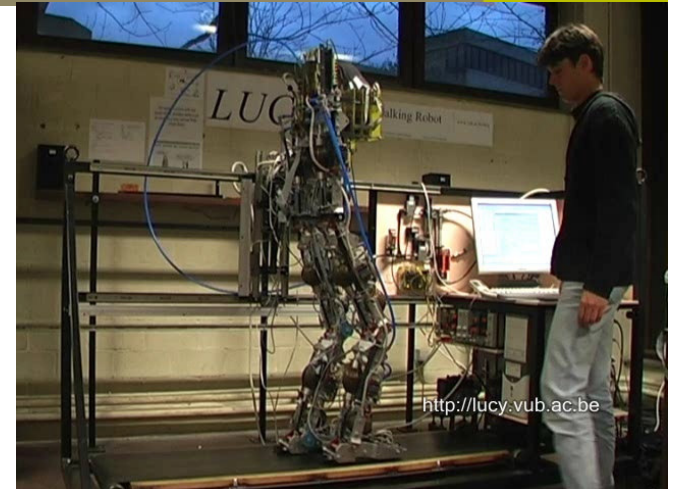
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# Antagonistic Controlled Stiffness



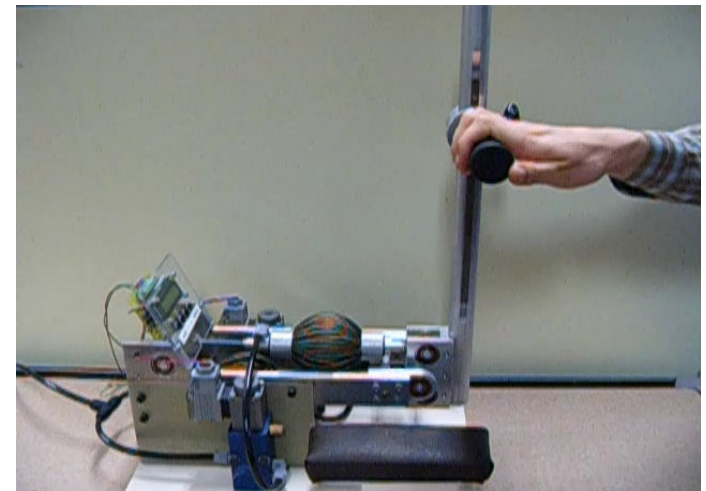
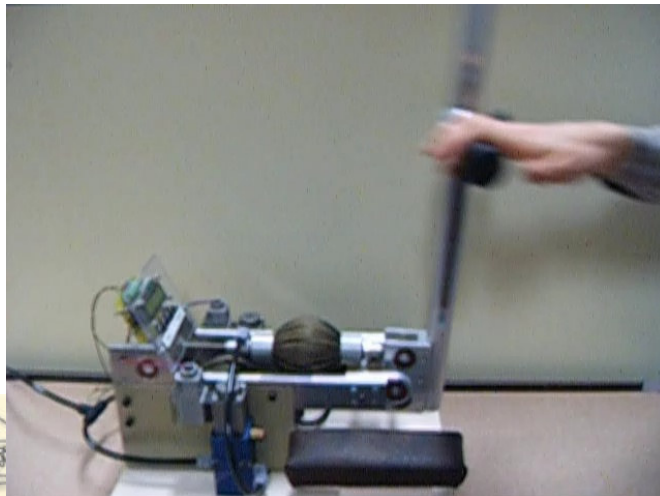
## Pleated Pneumatic Artificial Muscles



More compliant



More stiff

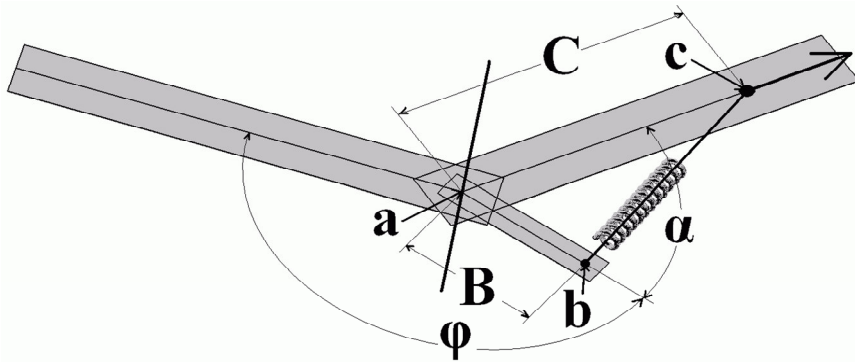






# Mechanically Controlled Stiffness

## MACCEPA Mechanically Adjustable Compliance and Controllable Equilibrium Position Actuator (R. Van Ham, VUB, 2006)



- straightforward mechanical concept

- $\phi \Rightarrow$  equilibrium position
- $P \Rightarrow$  joint stiffness

- linearized torque formula

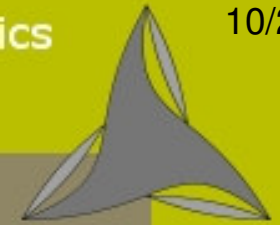
$$\begin{cases} T = \alpha \cdot \mu \cdot P \\ K = \mu \cdot P \end{cases}$$

- $\phi, P$  independent of actuator state



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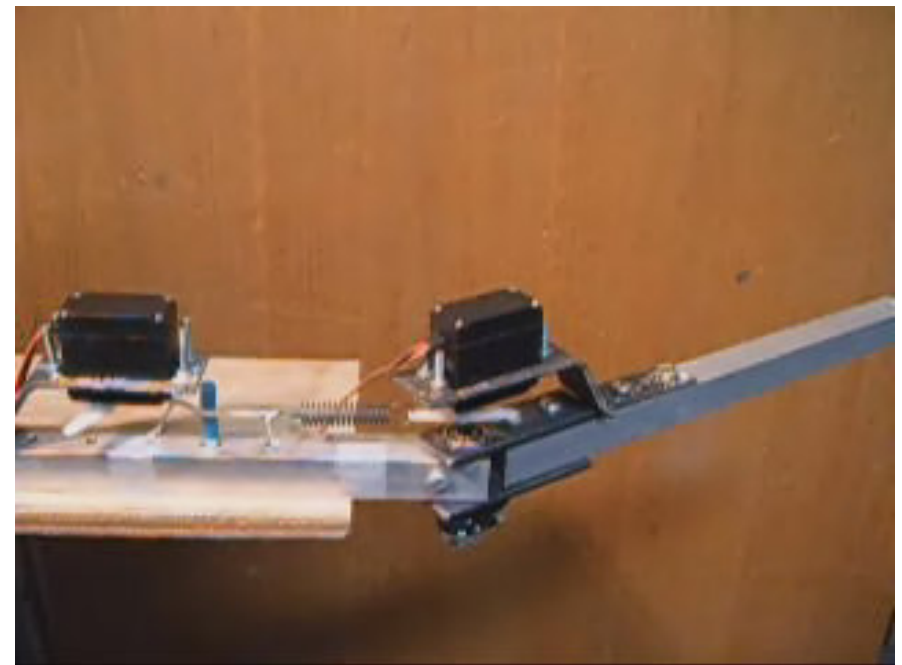
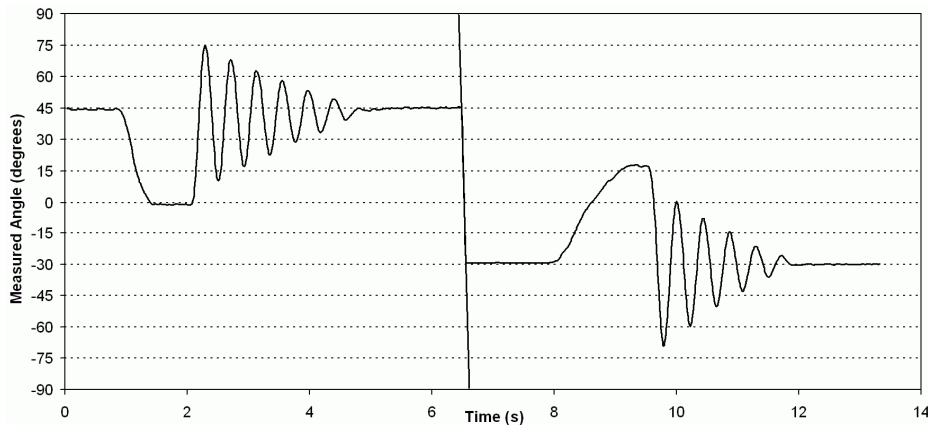


# MACCEPA: Changing Equilibrium Position

Torsion Pendulum → MACCEPA

$$f = \frac{1}{2\pi} \sqrt{\frac{\kappa}{I}} \longrightarrow f = \frac{1}{2\pi} \sqrt{\frac{\mu \cdot P}{I}}$$

$$T = \alpha \cdot \mu \cdot P \quad \mu = \frac{k \cdot B \cdot C}{|C - B|}$$



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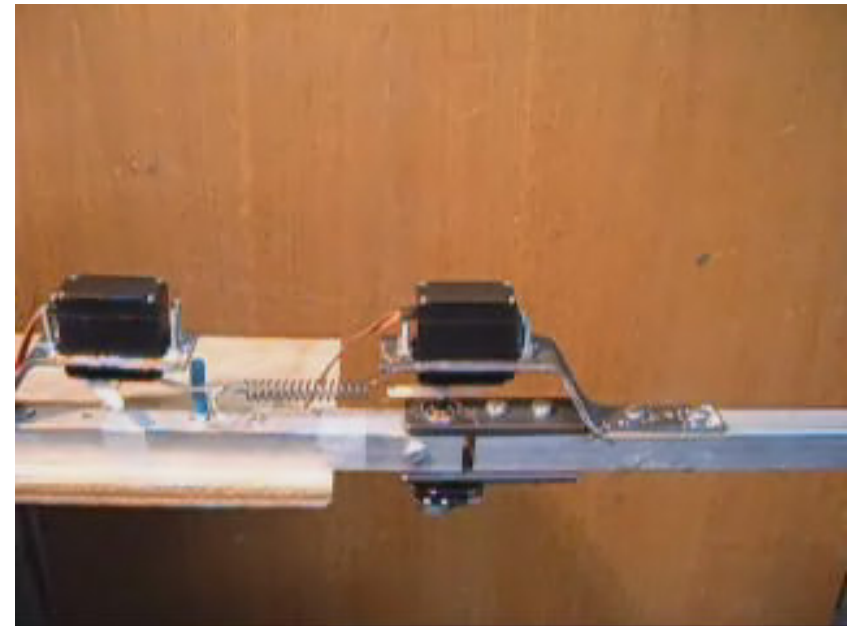
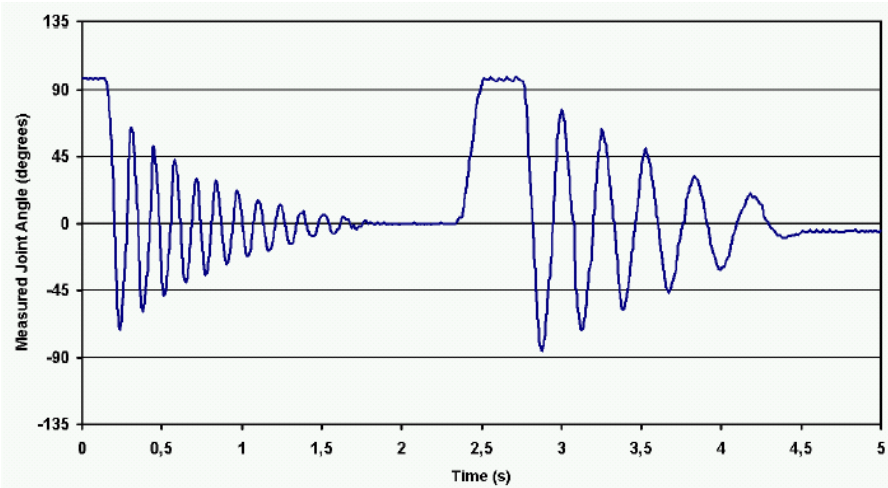


# MACCEPA – Changing stiffness

Torsion Pendulum → MACCEPA

$$f = \frac{1}{2\pi} \sqrt{\frac{\kappa}{I}} \longrightarrow f = \frac{1}{2\pi} \sqrt{\frac{\mu.P}{I}}$$

$$T = \alpha . \mu . P \quad \mu = \frac{k.B.C}{|C - B|}$$



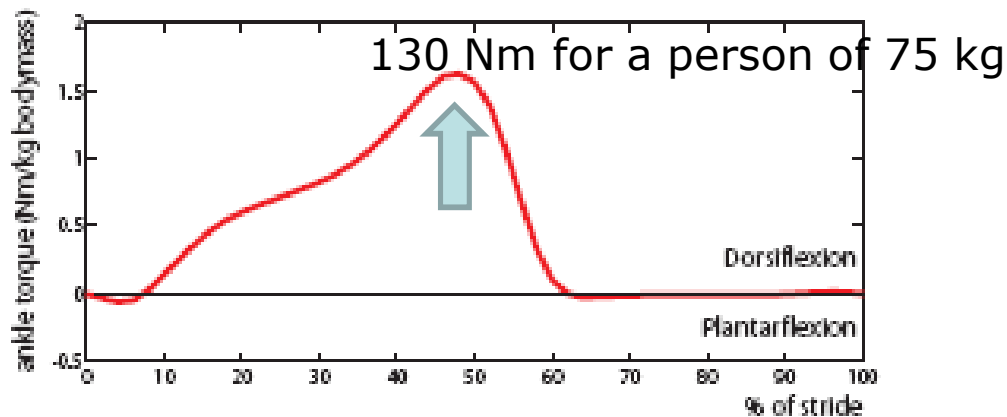
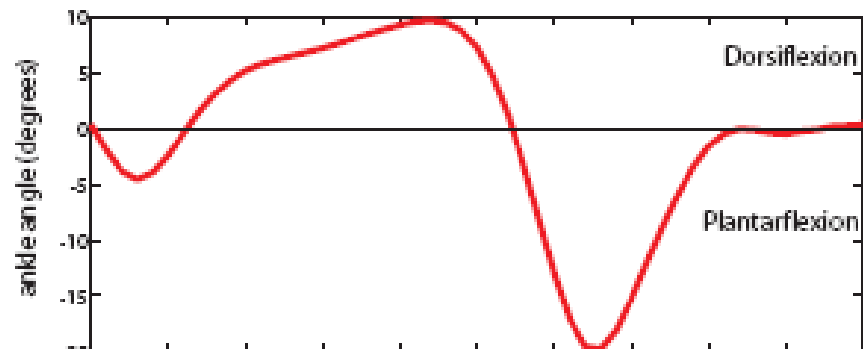
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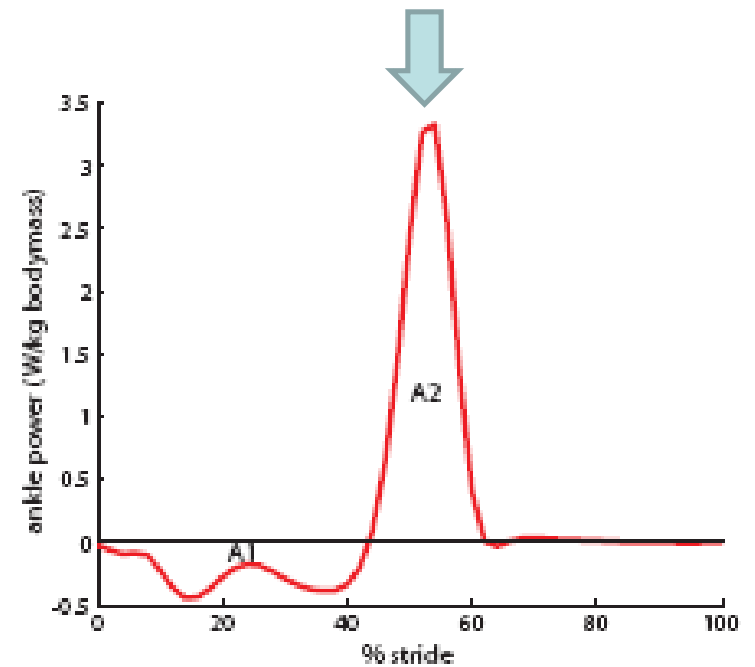
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# Normalised Ankle-data by Winter

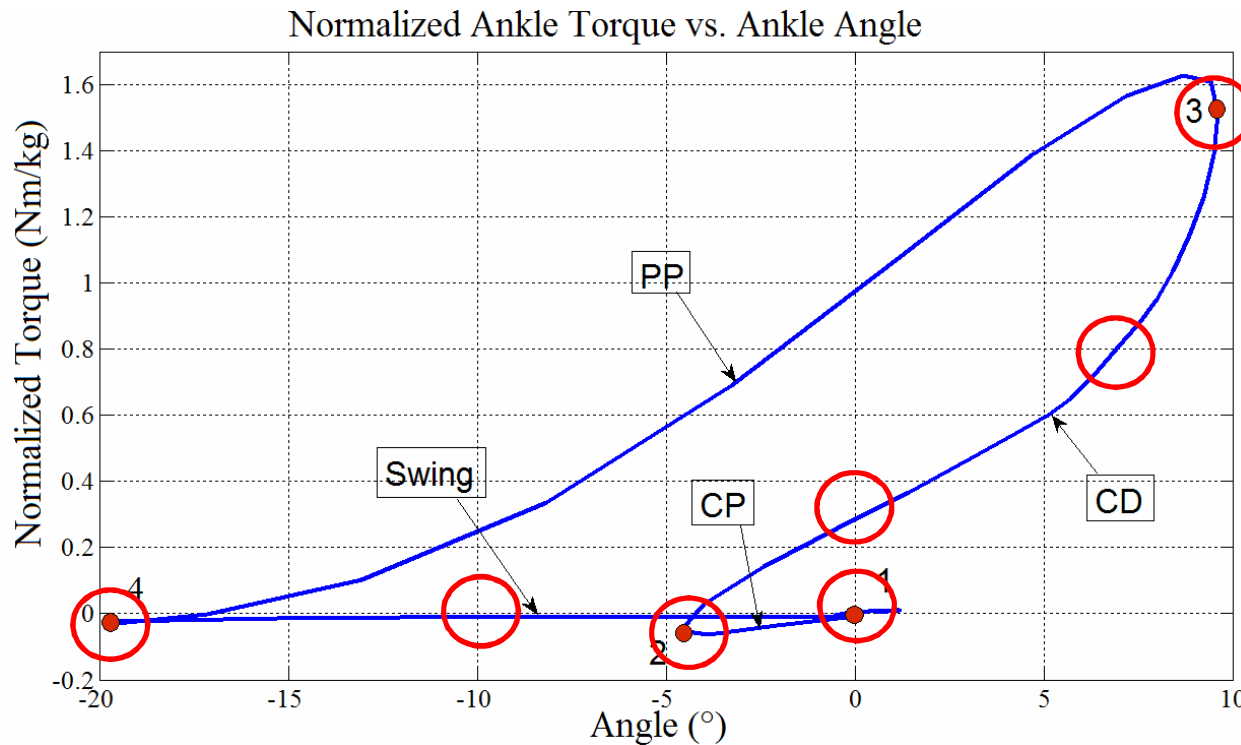


260 W for a person of 75 kg

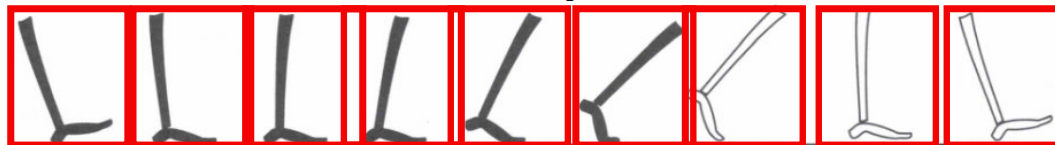




# Torque-angle characteristic of a human ankle

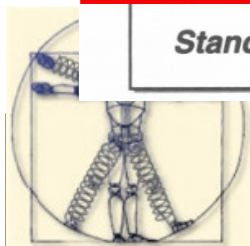


- 1 : Heel - Strike
- 2 : Foot - Flat
- 3 : Heel - Off
- 4 : Toe - Off
- CP = Controlled Plantarflexion
- CD = Controlled Dorsiflexion
- PP = Powered Plantarflexion



Stance

Swing



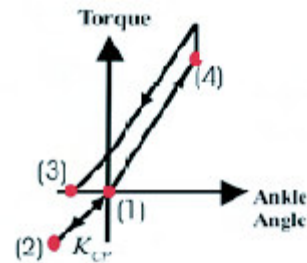
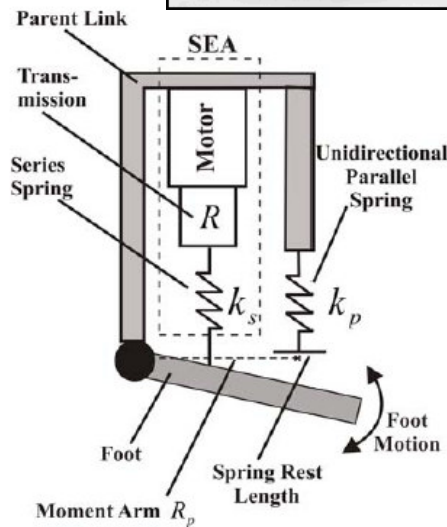
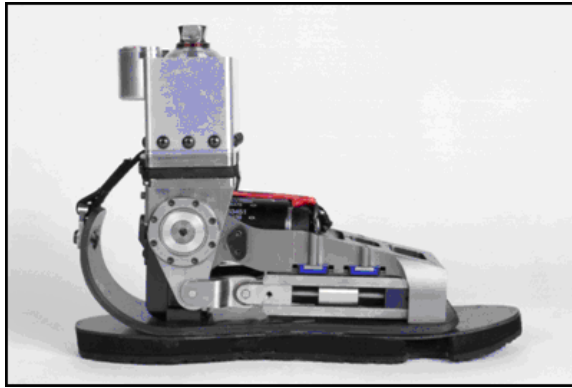
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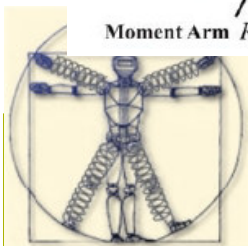
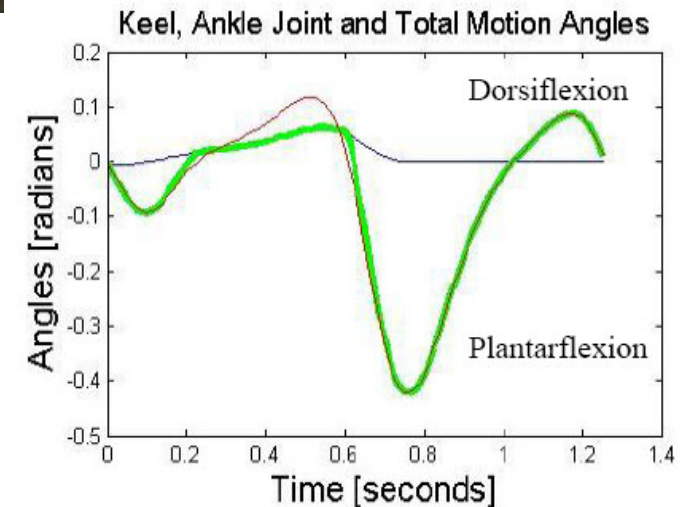
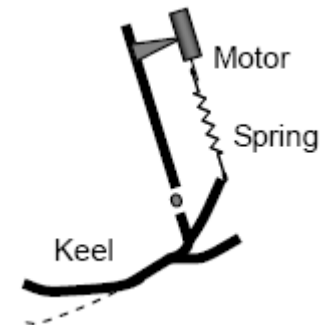
# Mimicking the human ankle: devices of Herr and Sugar

## H. Herr (MIT)



- (1) Heel Strike
- (2) Foot Flat
- (3) Toe Off
- (4) Start of Push-Off

## T. Sugar (Arizona State University)



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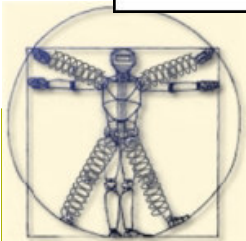
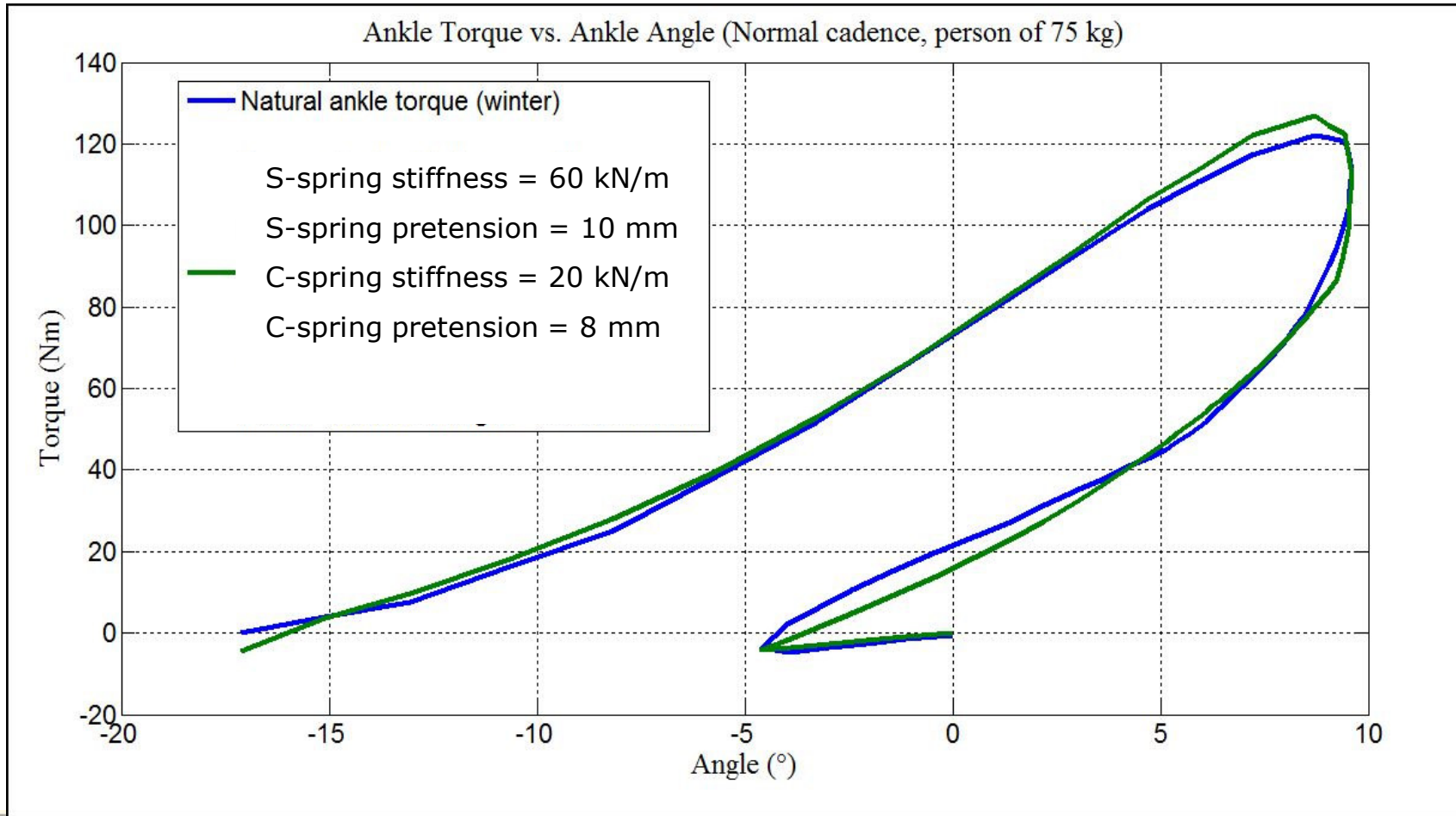
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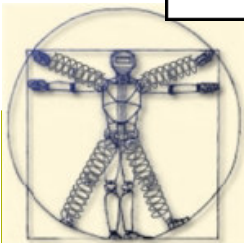
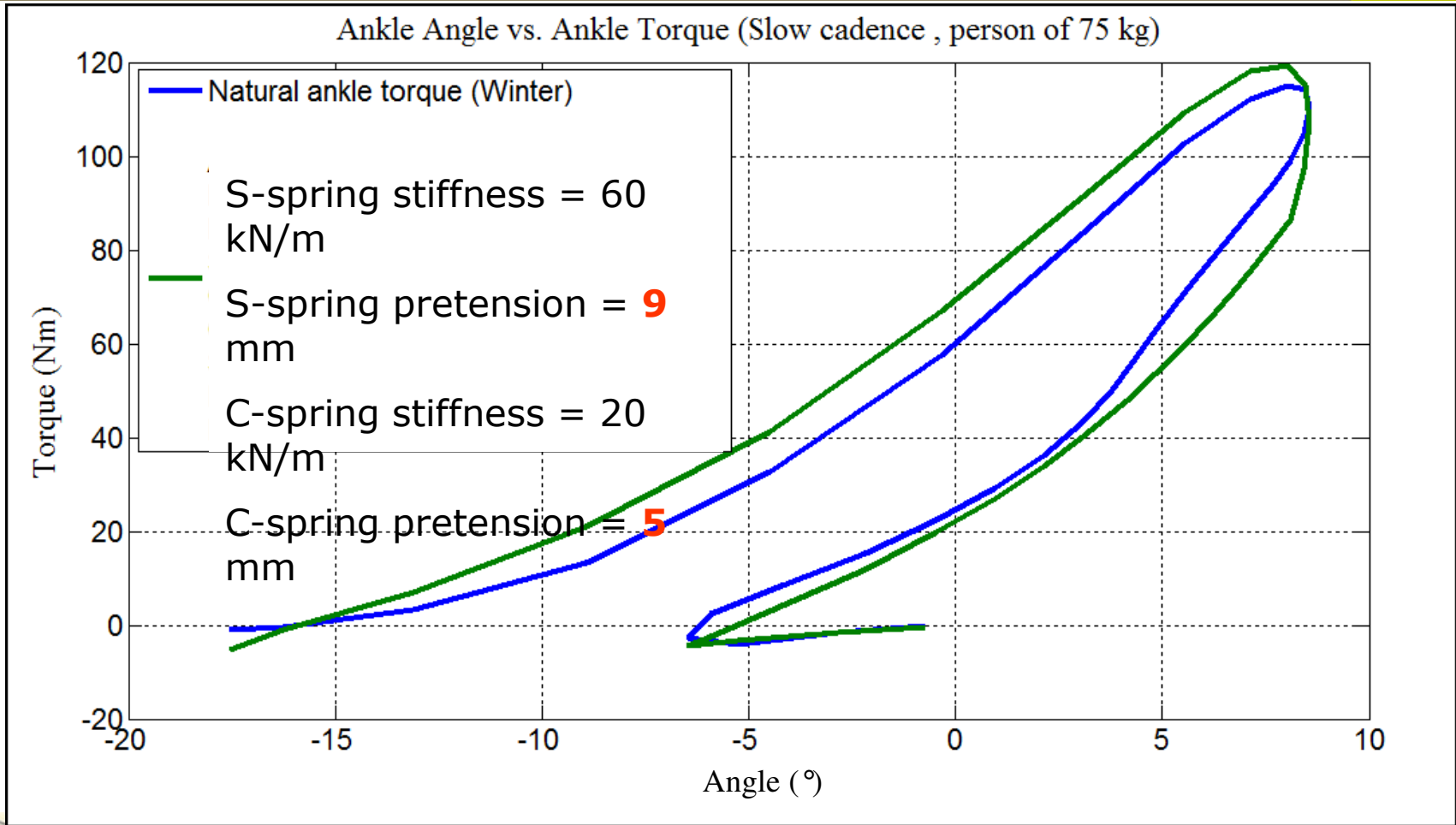


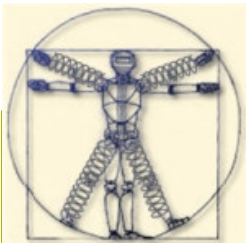
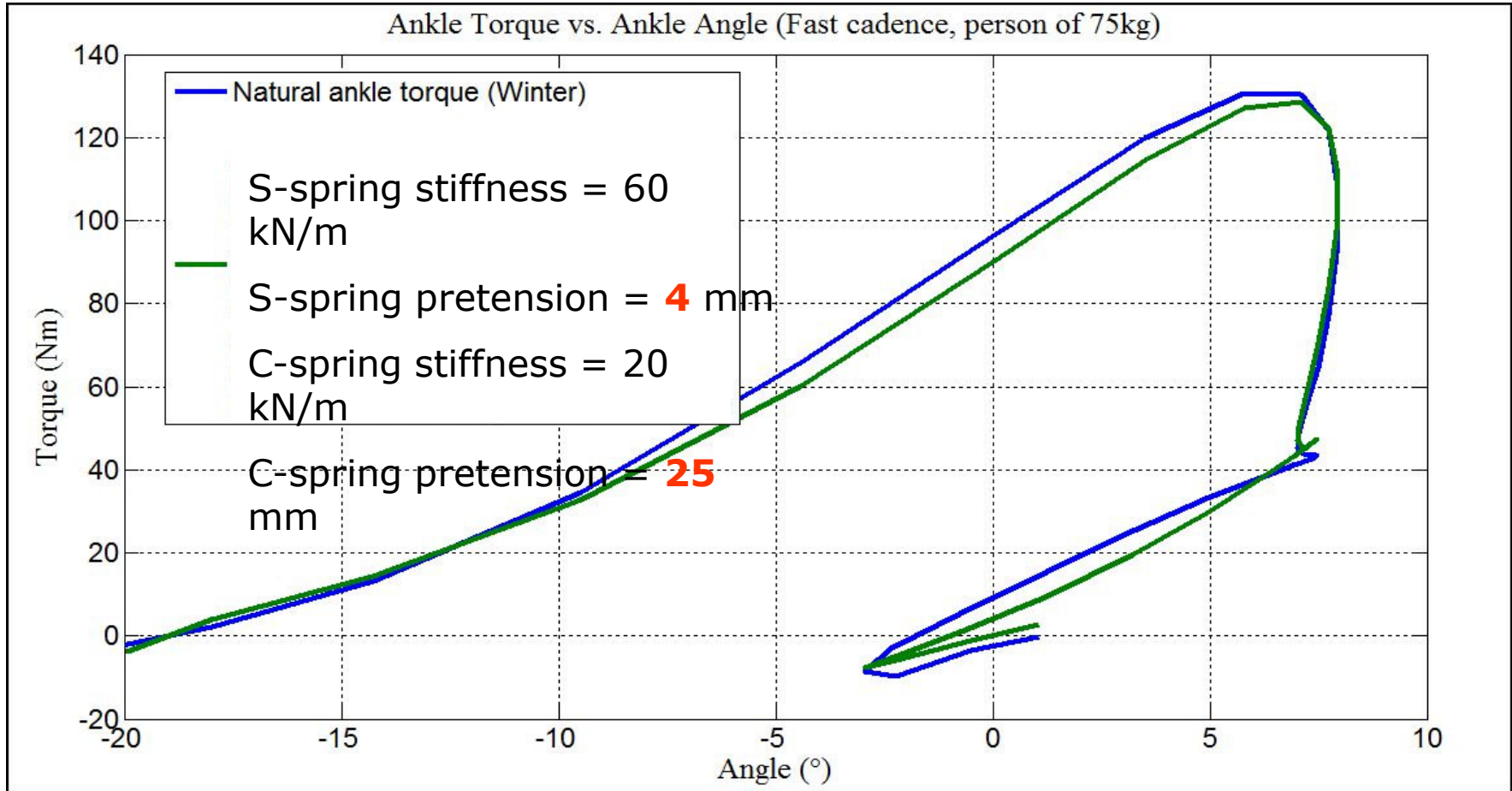
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Promising performance output for different step speeds

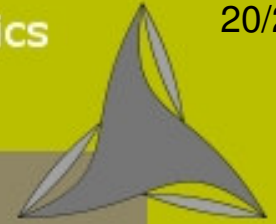
- Lithium ion-polymer battery : 200 Wh/kg
- Maxon RE40 150 W brushed DC-motor
- 22,19 J/step for normal cadence

<i>cadence</i>	slow	normal	fast
Required battery weight (in g) for 1,5h/day walking	177	282	463
run time (in h) with 1,5kg battery pack	13	8	5

- cfr. SPARKy : 21 J/step      8h



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## Conclusions

- Variable impedance actuators are able to reduce peak torque and peak power
- Variable impedance actuators allow to adapt to changing torque characteristics by adapting the compliance
- Negative work can be stored in a variable impedance actuator, and energy consumption can be reduced
- Impact is no problem
- These characteristics of variable impedance actuators are important in the development of efficient humanoid robots





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